

# Just-in-time Dosimetry using Positron Emission Tomography

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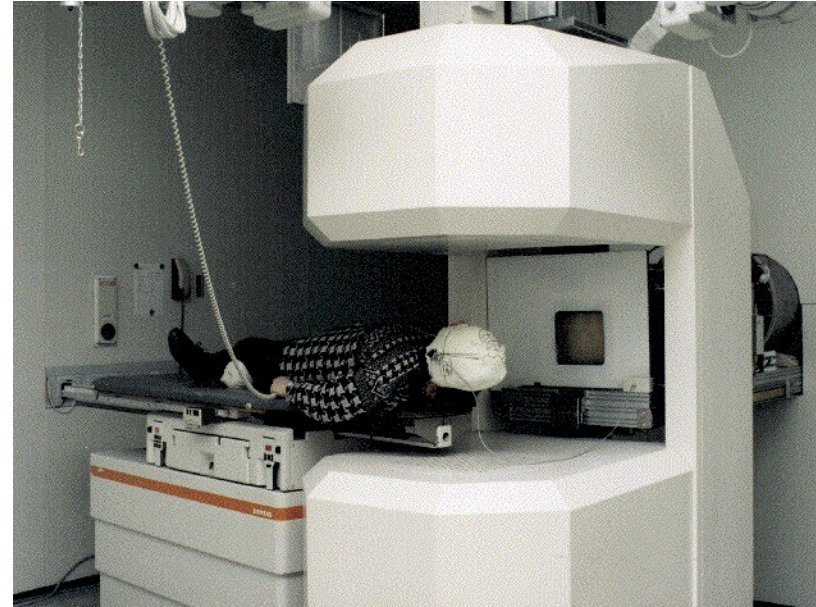
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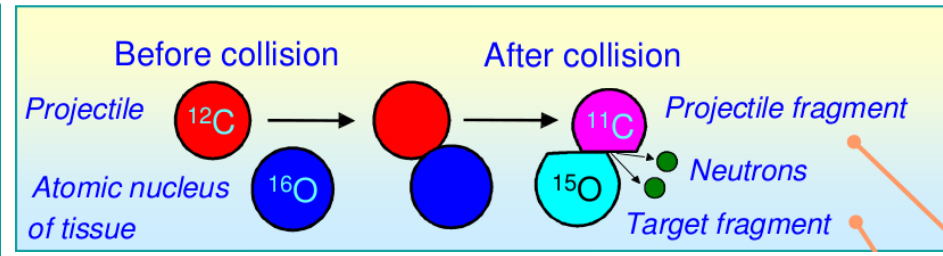
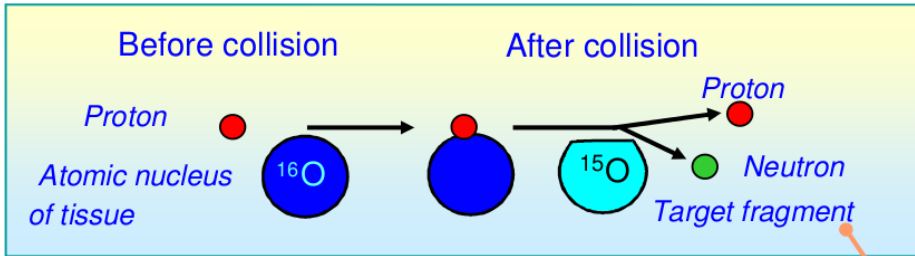
# Medical in-beam Positron Emission Tomography (PET)

## Radiation treatment for head tumor

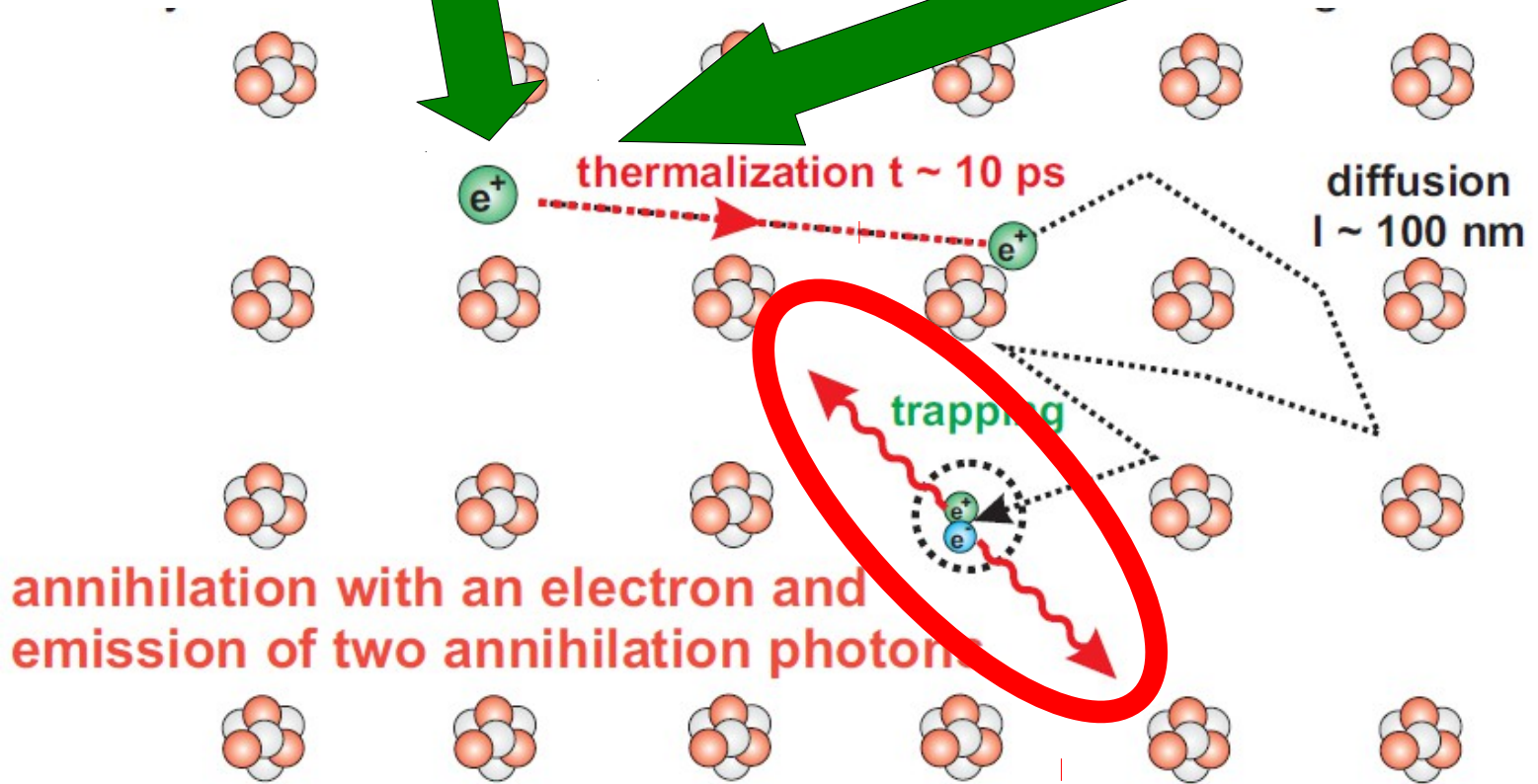
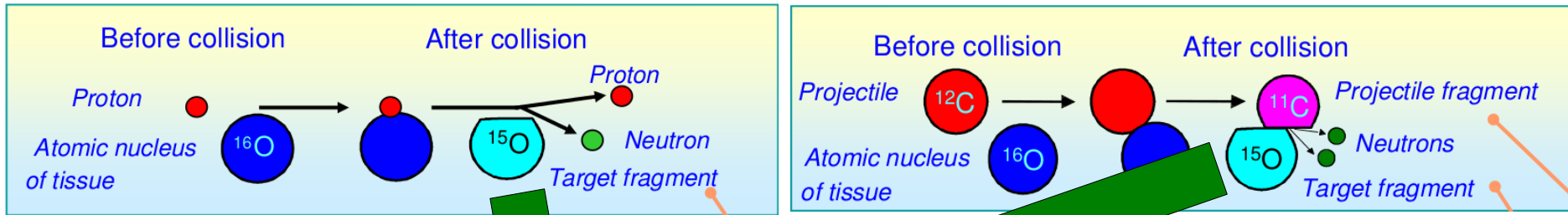
- Protons / heavy ions
- Multiple irradiation sessions [weeks]
- Sessions possibly fractionized [1 hour]
- **Goal: Dosimetry imaging at the time of irradiation**



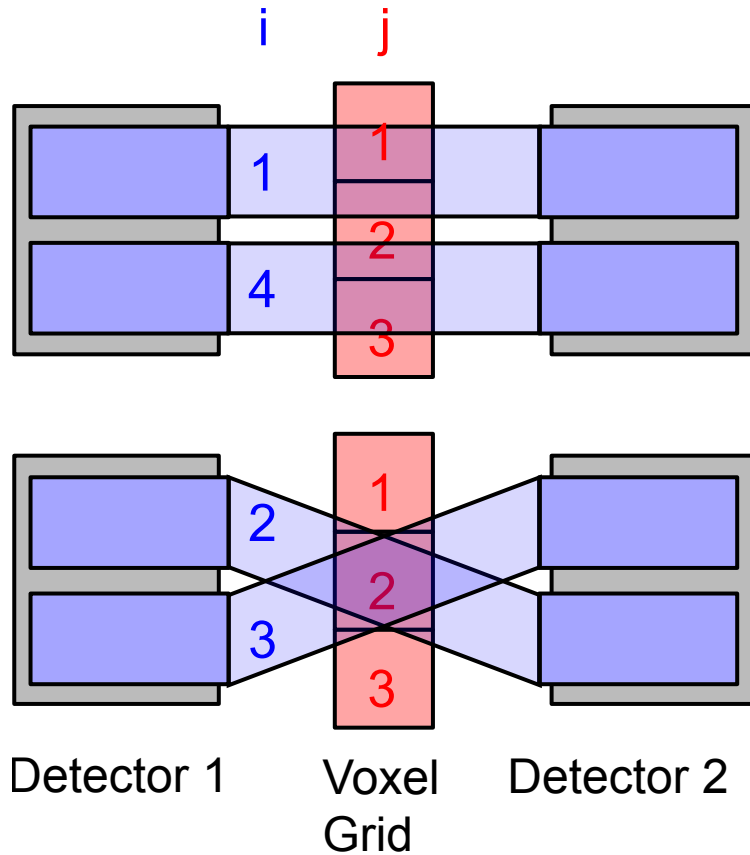
# Signal originates from positron-electron-annihilations



# Signal originates from positron-electron-annihilations



# Coincidence detection



- Annihilation photons detected in pixel detectors
- „Event“: Coincident detection in two different detectors
- Pixel pairs = lines of response (LOR)  
→ here: blue stripes with indices  $i$

# Detector systems

## Numbers:

- Typically ~100 pixels per detector
- Up to ~10.000 pixels in total
- Up to ~10e5 .. 10e6 LORs
- Maybe additional LORs through translation, rotation

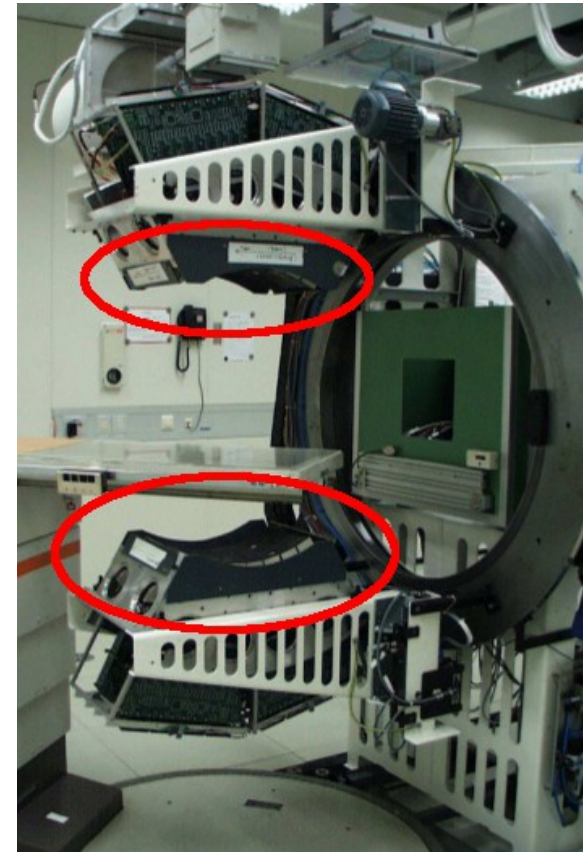
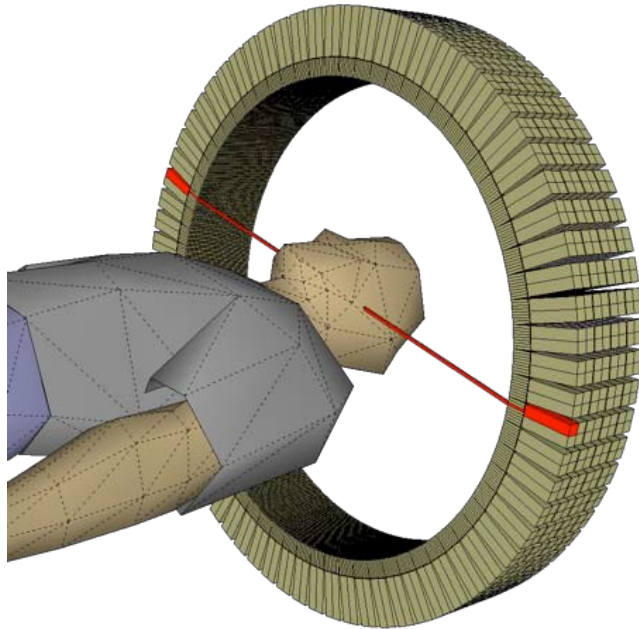
## Remember: Dosimetry wanted

- Number of measured coincidences from a volume ~ number of beta(+) decays
- That's **activity**
- Dose applied along the way with dependence on tissue properties
- **Dose** is not activity
- **Wanted quantity is not easily correlated to the signal!**

# Detector systems



Scanner-Ring



In-beam PET-Scanner @GSI



# Data



- Roughly some 10 MB / min
- Total: 100 MB .. 1 GB
- That's relatively few → poor counting statistics
- Tunable - to a degree - by choice of detector
- Depends on total irradiation!

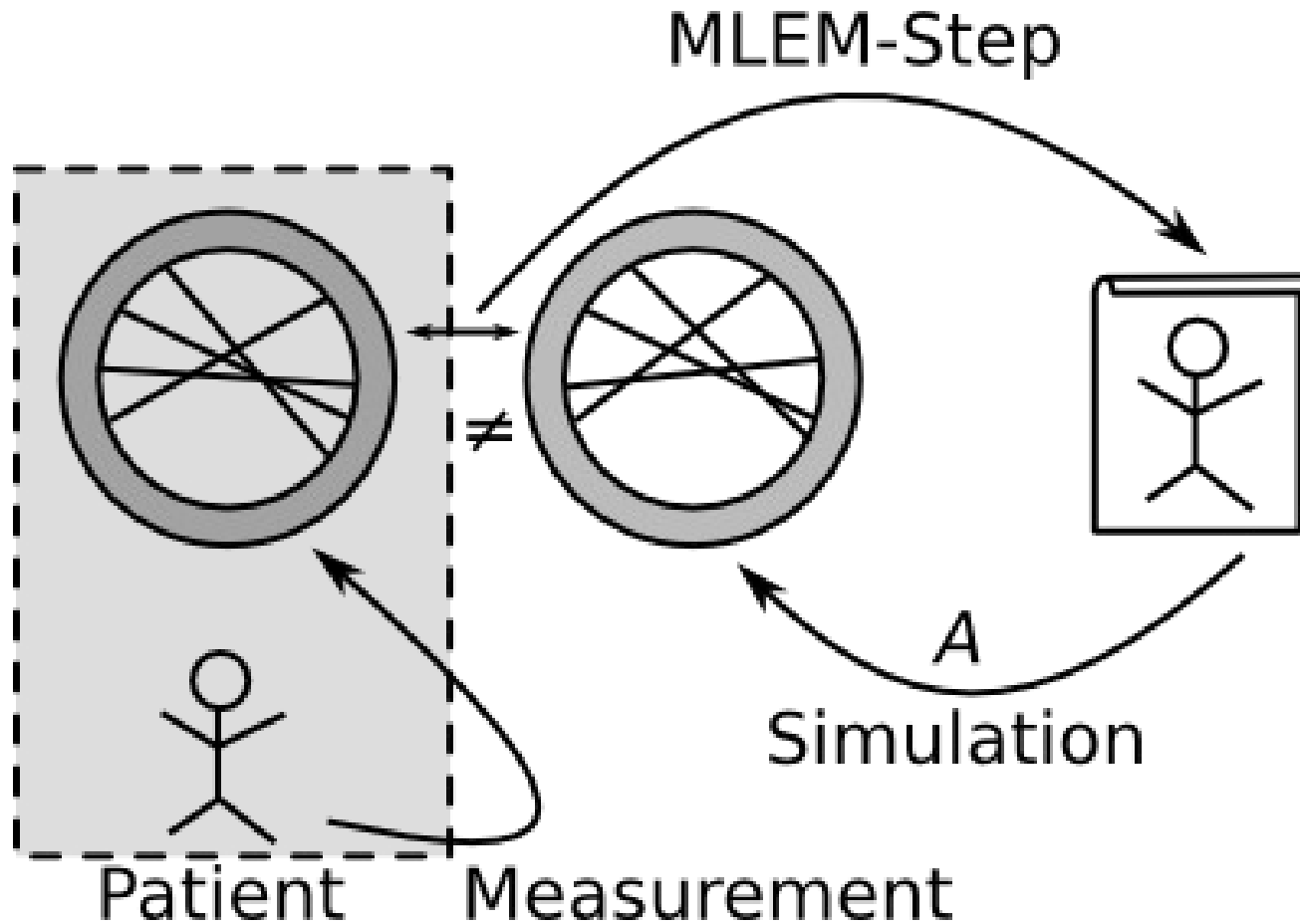


# Implications for the reconstruction

## Challenging!

- Direct methods hard / impossible to employ
- Dose non-trivially correlated to measured „activity“ signal
- Use as in-situ imaging for feedback: Reconstruction should take no longer than **a few minutes**

# Iterative reconstruction is method of choice

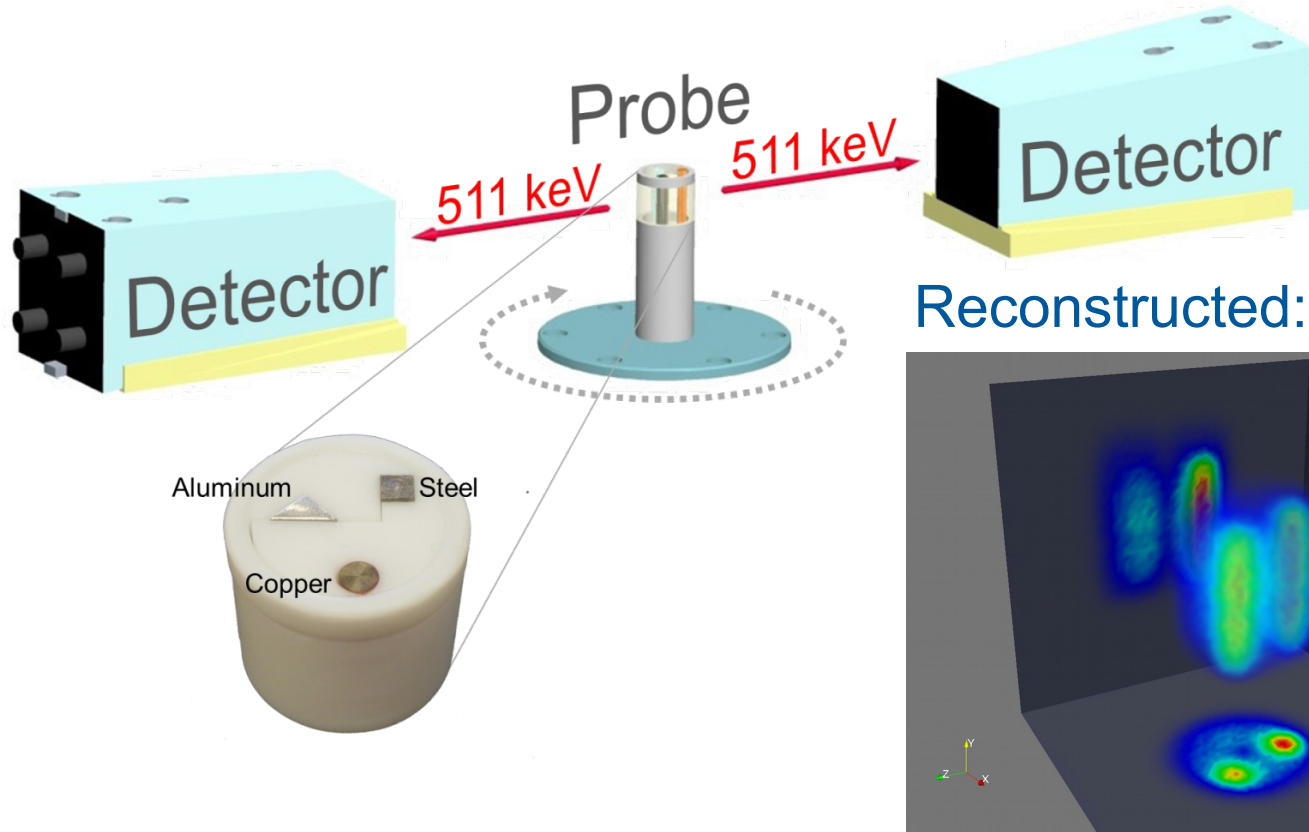


# Iterative reconstruction is method of choice

## Maximum Likelihood Expectation Maximization (MLEM):

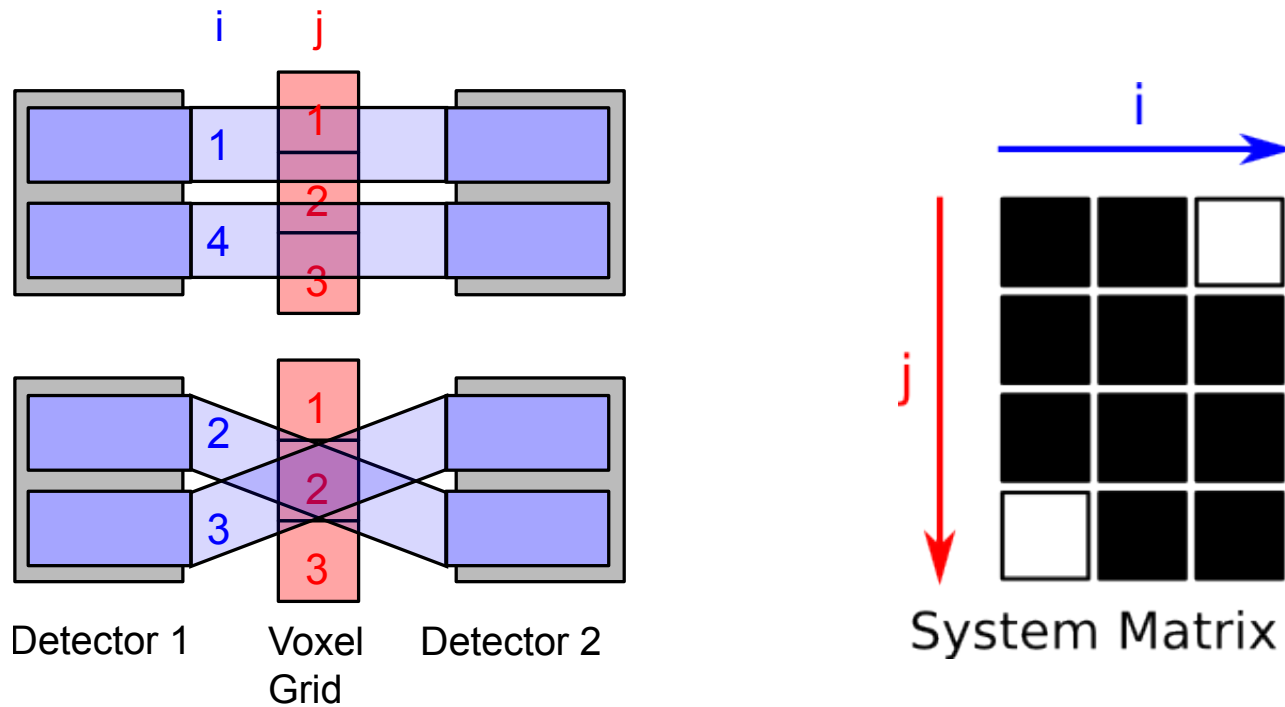
- Statistical approach
- Uses forward projection, can linearly be described as **System Matrix (SM)  $A$**
- Pro: Put any knowledge into SM → dosimetry
- Roughly 50 iterations necessary

# Plastic and metal phantom as an exemplary model system



- $180 * (13 * 13) * (13 * 13)$  LORs  $\approx 5,000,000$  LORs  
 $\approx$  **50 MB input data**
- $64 * 64 * 64$  voxel  $\approx 250,000$  voxel

# Estimation of SM size



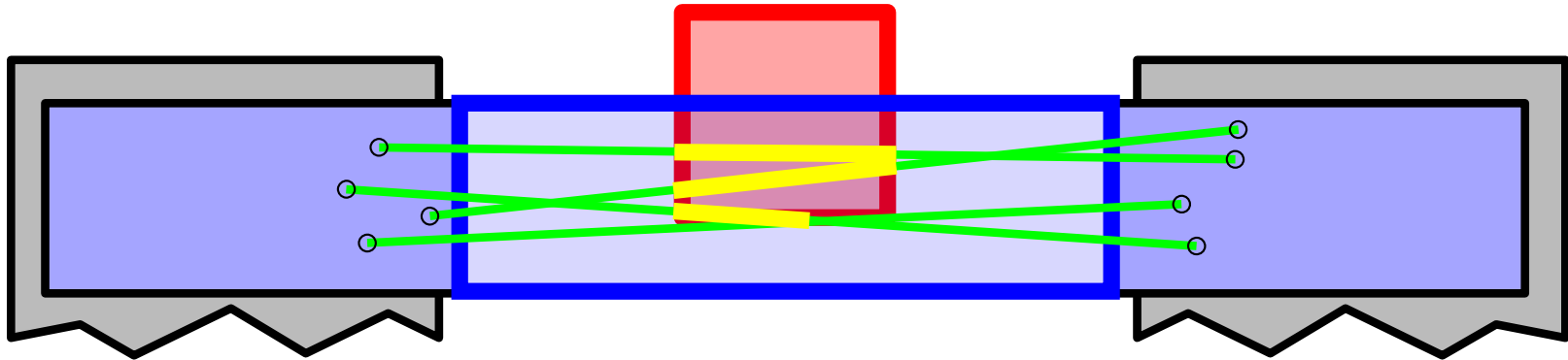
- SM is thinly occupied, ca 5 %
- $6.7e10$  non-zero SM elements = **500 GB**

# Reconstruction becomes an HPC problem

## Time for model reconstruction:

- 1 GPU: 10 h / 1 reconstruction step
- Note: **500 GB SM - Big Data even though input was just 50 MB!**
- Let's look into parallelization ...

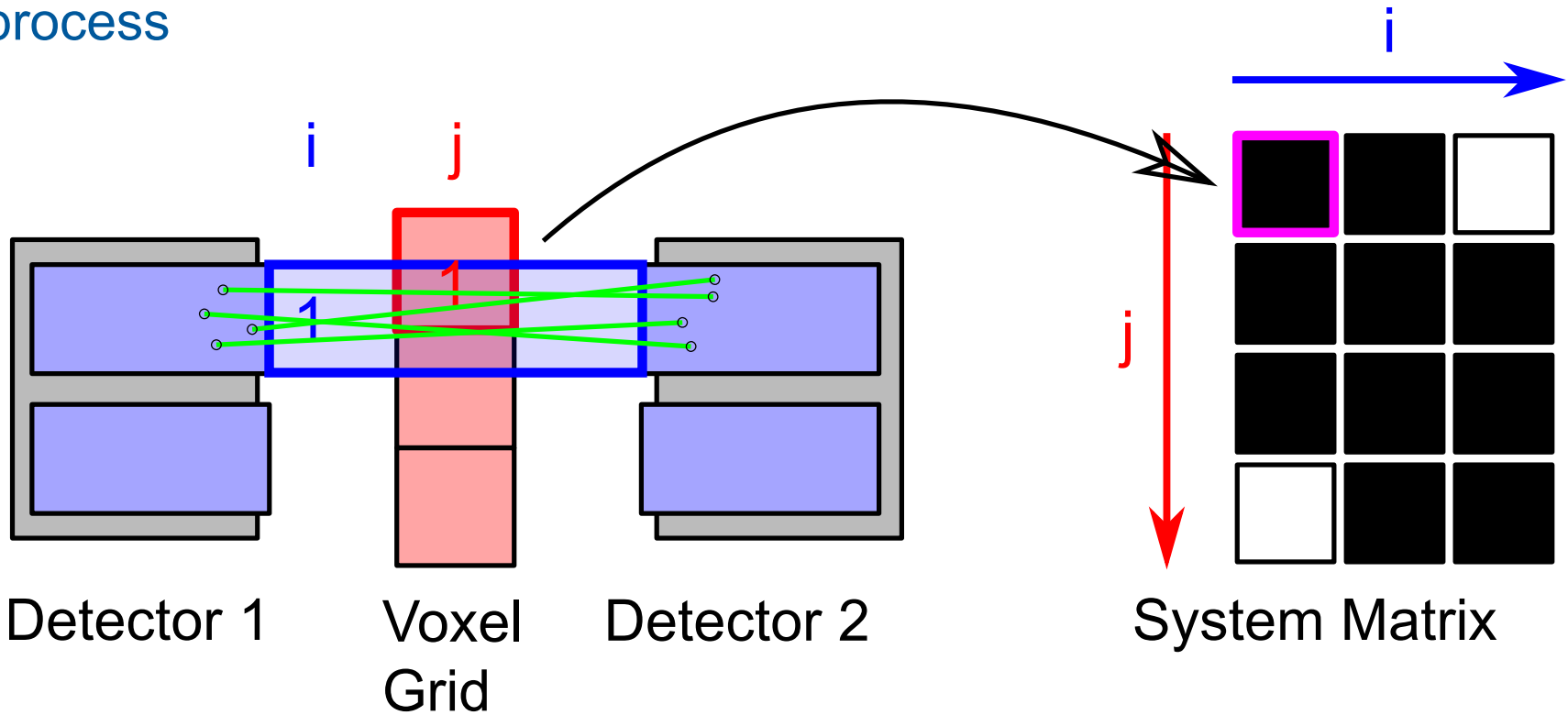
Calculating the system matrix is simulating the measurement process



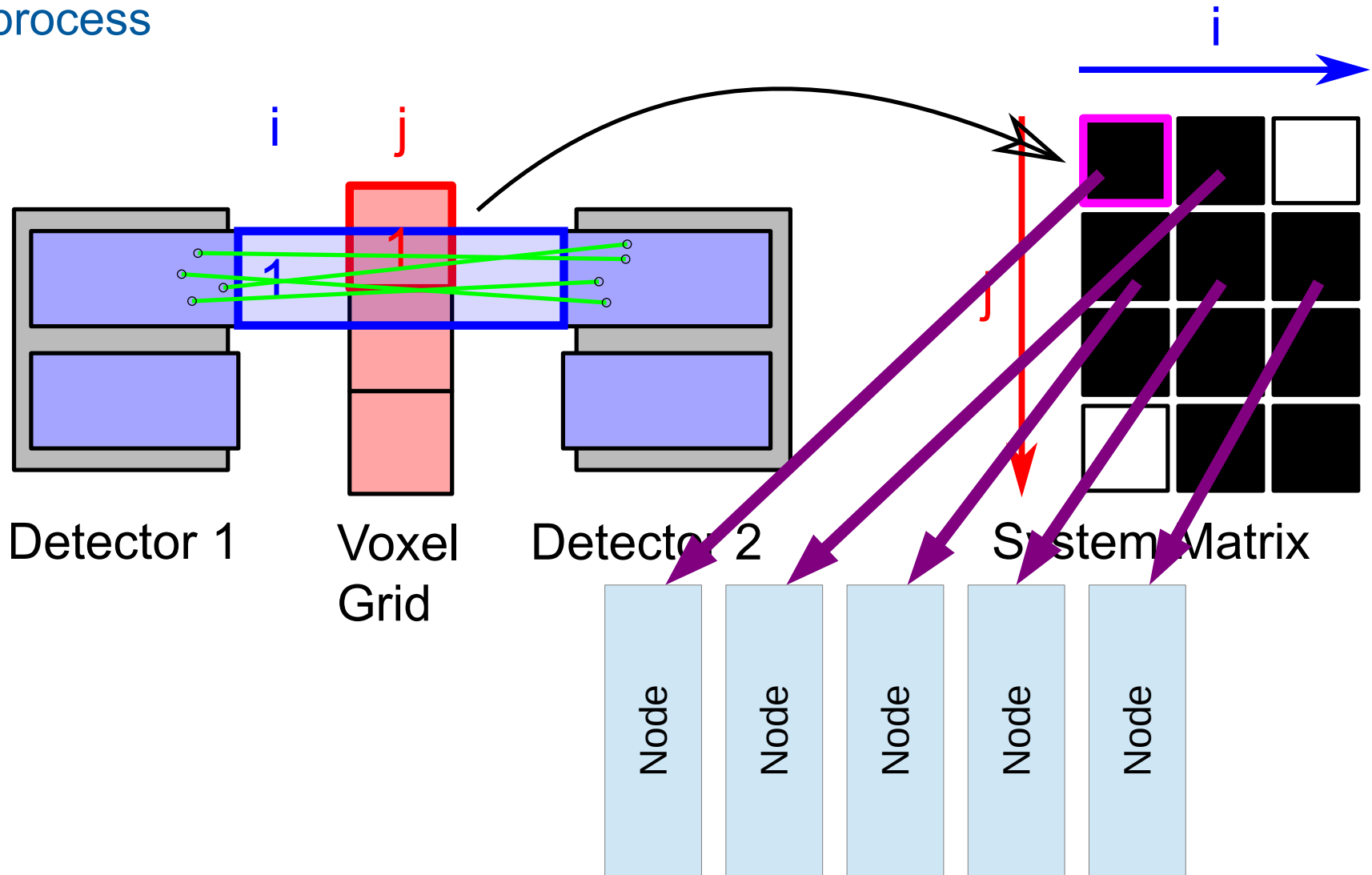
**Put knowledge about measurement process here!**



# Calculating the system matrix is simulating the measurement process

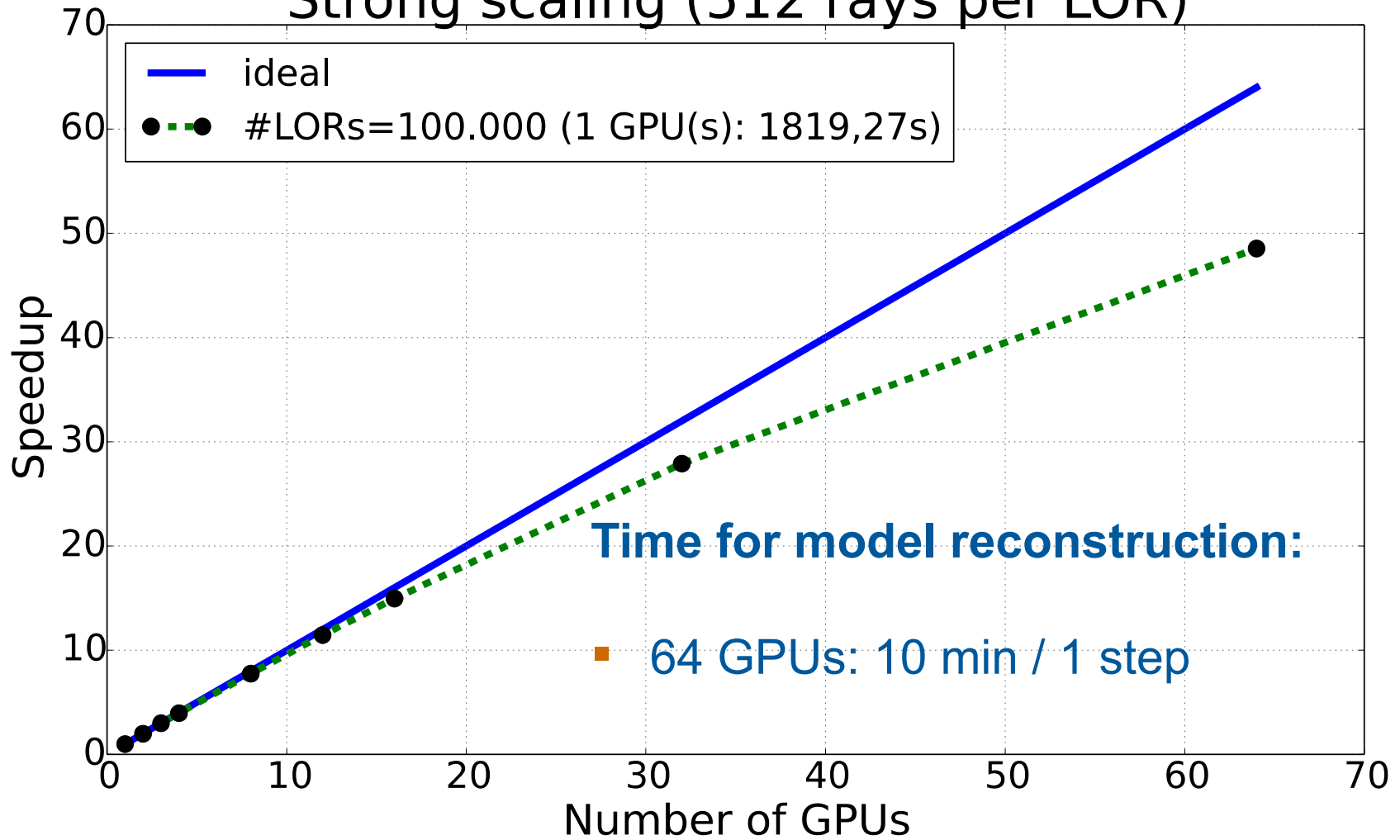


# Calculating the system matrix is simulating the measurement process



# First step done: Whole reconstruction runs parallelly

## Strong scaling (512 rays per LOR)



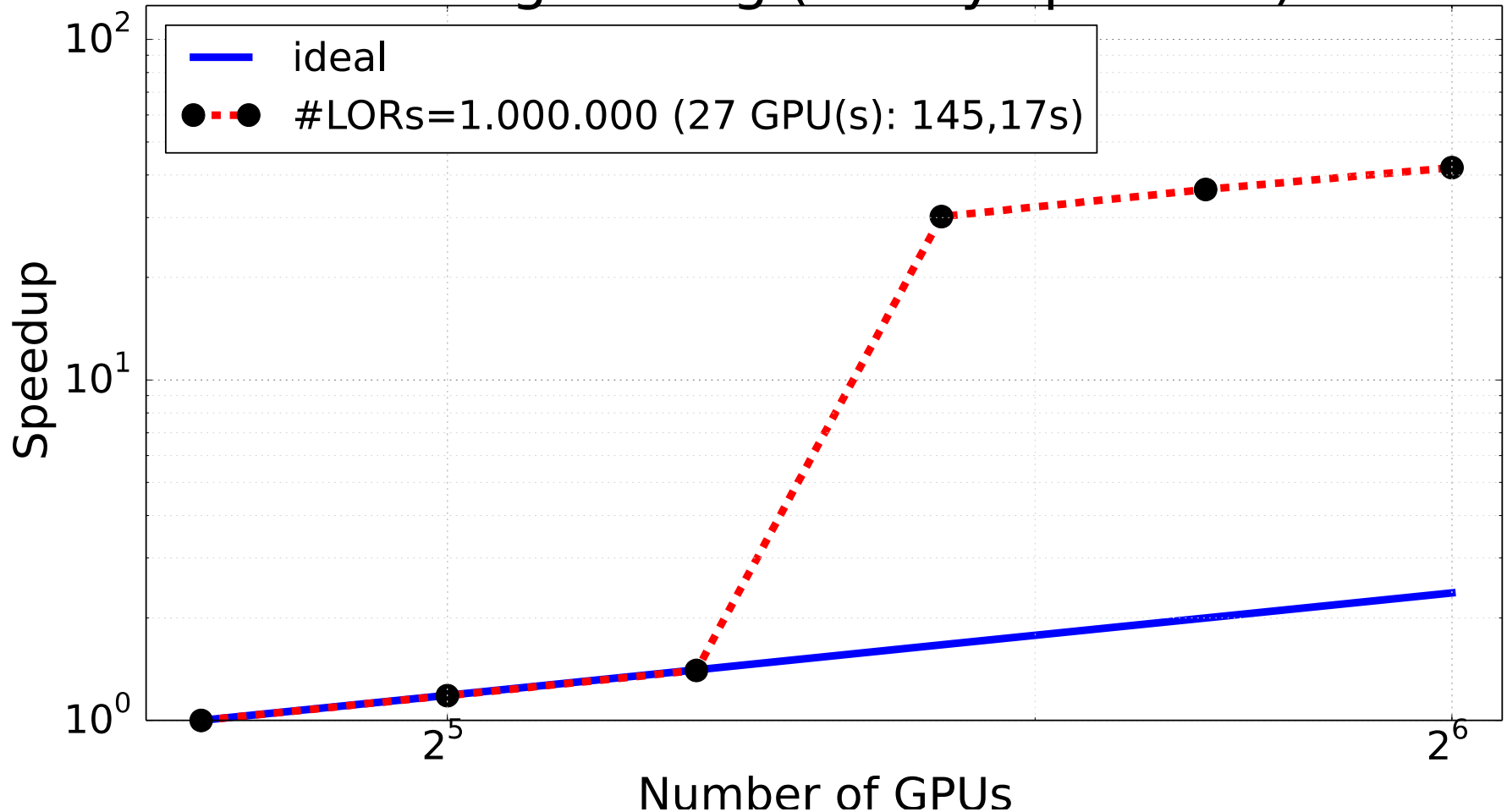
# Keep the system matrix!

## Good assumption:

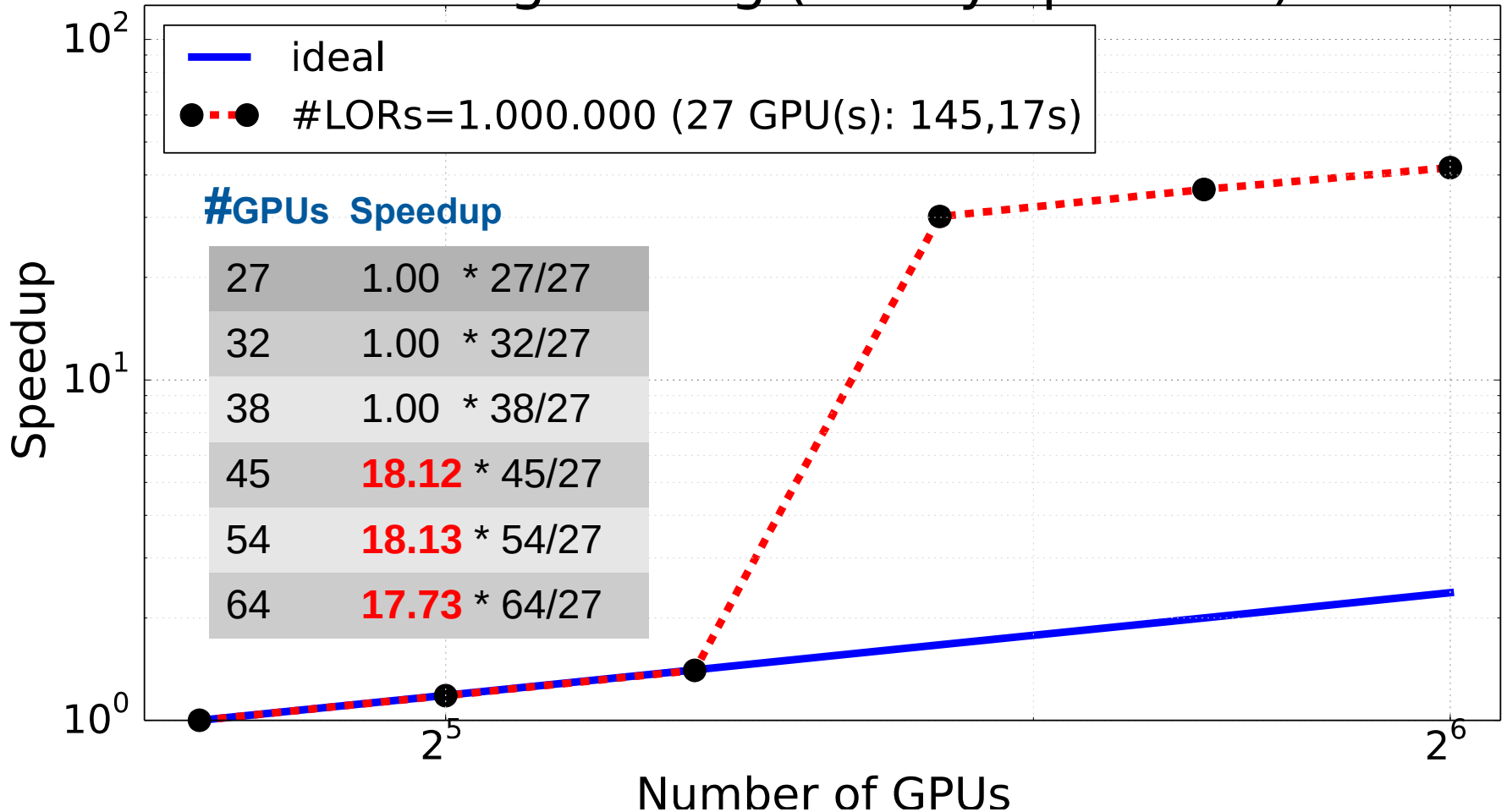
- Rigid, unchanging target → **constant SM**
- Adoptable to patient
- Use CPU mem for saving the SM between steps

With system matrix in CPU mem

## Strong scaling (32 rays per LOR)



# Strong scaling (32 rays per LOR)



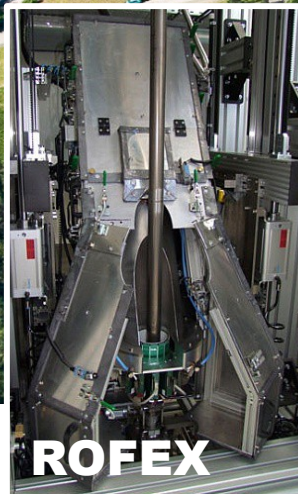
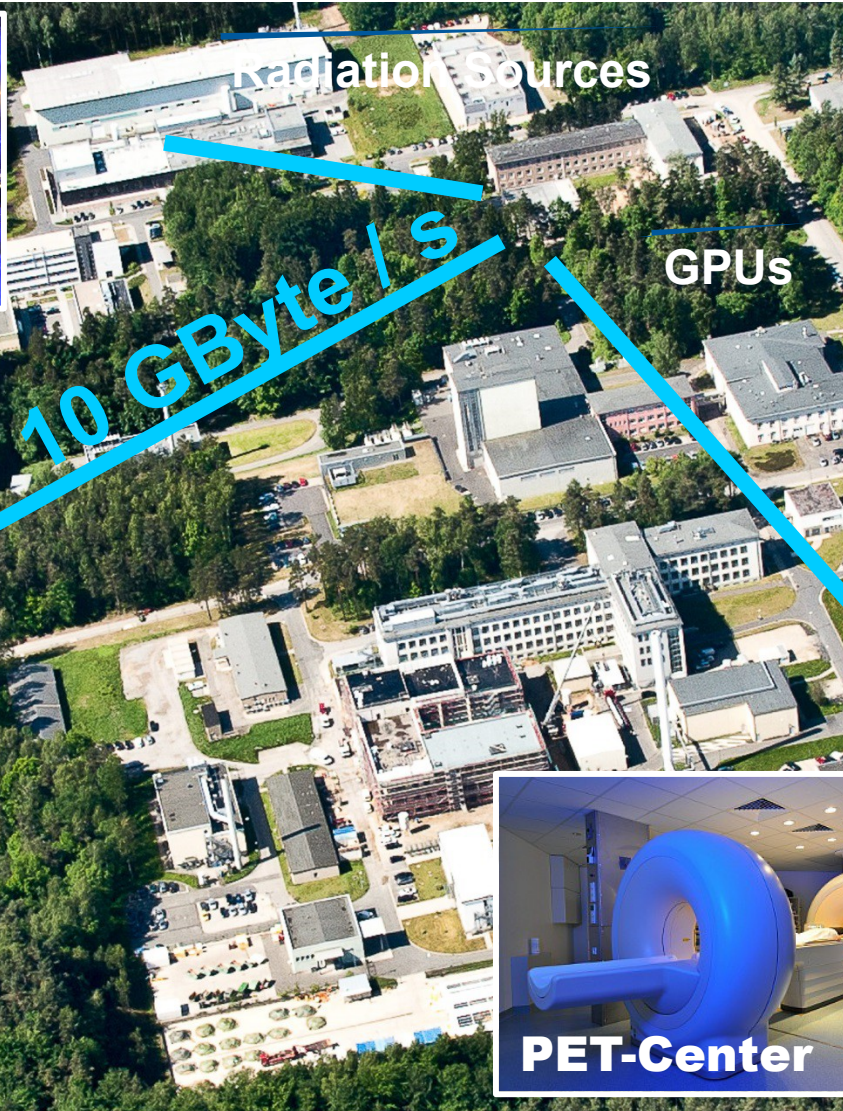
- Keep SM *on GPU*
- Implement caching techniques (CPU, GPU)
- Porting to Alpaka, Graybat :-)

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# Central GPU-accelerated realtime Data Analysis @ HZDR



**GPU CENTER OF EXCELLENCE**

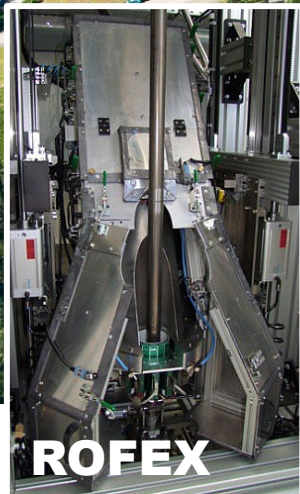
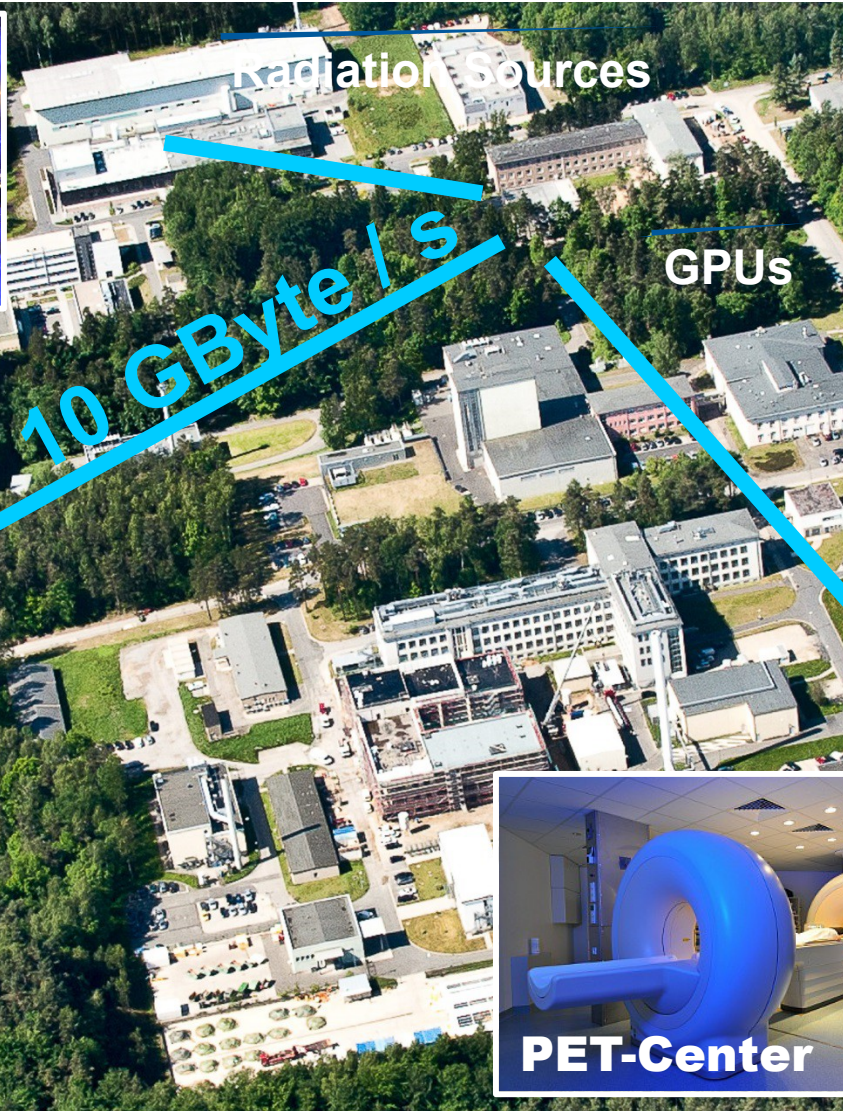


DRESDEN concept



**HZDR**

# Central GPU-accelerated realtime Data Analysis @ HZDR



## 9 compute nodes in total, 1 node equipped with

- 4 × NVIDIA K80 (24 GB) @ full PCIe 3.0 Bandwidth
- 2 × INTEL XEON 8-core
- 256 GB memory ( $\sim 2.7 \times$  GPU memory, 16 GB / core)
- Mellanox 56 GB/s FDR